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Transport device for sterile media

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DESCRIPTION

The invention relates to a device for transporting sterile fluids, e.g. Ringer solution, such as are employed for example in water-jet surgery.

15 In the area of water-jet surgery – this is an especially important example – in general the following requirements must be met:

- The sterility of the fluid must be ensured, because it not only comes into contact with a patient's body but also to
20 some extent remains in the body;
- the required flow and/or the pressure needed for such flow must be substantially constant and reproducibly adjustable, to achieve a reproducible effect on the tissue;
- the person operating the device must be free to select the
25 duration of an individual activation with constant flow;
- containers for the fluid should be available in differing sizes, so that for a particular application the amount required can be kept in reserve, with no need to exchange the container during an application on one hand and, on the
30 other hand, without leaving a too-large container only partially emptied;

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- it must be possible to begin and end the activation of the instrument substantially without delay, i.e. the pressure must build up rapidly and no drops may appear post-activity;
- 5 - it must be possible to exchange applicators with no problems.

Surgical water-jet cutting devices and associated systems for pressure build-up are known per se. One technical solution to the problem of keeping the operating fluid completely sterile,
10 namely by preventing it from coming into any contact with parts of the pump mechanism, is disclosed by the document DE 42 00 976 C2. With this known solution, however, the user has available only a specific quantity of the fluid medium, because it is contained in a previously prepared cartridge. Once this
15 has been opened, any content that remains cannot be put to further use, regardless of how much or how little has been extracted during the actual operation. The residue must be discarded. The maximal size of the reservoir in this known arrangement is crucially determined by the dimensions of the
20 device. When a small device is desired, it can easily happen that the reservoir must be exchanged during the operation, which constitutes a disturbing interruption of the procedure. Furthermore, the reservoir must be pressurized as a whole, so that there is a dependence on the sizes that are available for
25 the reservoir.

Sterile filters, which allow nonsterile transport in that they filter out any germs that could have entered the cutting medium from a nonsterile transport device, present various disadvantages. One is that the effort of maintenance is
30 considerably increased, because the filters must be exchanged at specified time intervals. Furthermore, filters tend to inhibit the flow behavior. In the case of high pressures, inserted sterile filters are suitable only with some restrictions, because when the instrument is turned on and off

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they are subjected to major changes in flow and thus also interfere with the required rapid pressure build-up.

It is the objective of the invention to disclose a transport device for sterile fluids that simplifies and improves its usability in the operating theater.

This objective is achieved by a transport device for sterile fluids to transport a sterile medium from a reservoir or similar source to a surgical instrument, in particular an instrument for water-jet surgery or a similar consumer apparatus, which comprises a piston pump or similar volumetrically transporting pump, with a suction cycle to draw the medium in and an output cycle to eject the medium, and which furthermore comprises conduits and valve means to connect the pump to the source and to the consumer, as well as drive means to drive the pump, the drive means being constructed and connected to the pump in such a way that the suction cycle is shorter than the output cycle. Alternatively, the pump can comprise three or more pump chambers, which are actuated in such a way that the pump cycles overlap.

In the case of the first alternative the pump preferably comprises at least one first and one second piston/cylinder unit or similar pump chambers, which can be controlled in a push-pull manner so that the suction cycle in the first pump chamber is shorter than the output cycle in the second pump chamber, and conversely. As a result, only two pump chambers suffice to ensure production of a continuous flow.

The drive means are preferably constructed such that the output cycles overlap one another. This ensures an especially uniform flow, with no need for storage vessels or the like.

Each drive means is preferably constructed such that the medium is supplied to the consumer with a substantially constant

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pressure and hence a constant transported amount. This considerably enhances usability.

Preferably the pump is releasably connected to the drive means. As a result a "sterile device part" can be separated from an
5 "unsterile device part" that could only be sterilized with extreme effort.

In this embodiment it is especially advantageous for the pump and/or the conduits to be constructed, preferably together with the valve means, as a "disposable unit". Thus for each
10 application a "set" consisting of pumps, the conduits and the necessary valve means is connected on one hand to the reservoir for the medium to be transported and on the other hand to the surgical instrument, and is then coupled to the drive means. After use this set as a whole is discarded. In this way
15 complete sterility can be ensured along with simple manipulation, because the set can be sterilized by the manufacturer in a simple manner.

For the drive means various alternatives are possible. For instance, for each pump chamber a separately controllable drive
20 motor can be provided, so that the velocity profile for the individual pump chambers can be set as desired with little effort, by employing an appropriate electronic control system (e.g., by using stepping motors). Alternatively (but in some cases also in addition) the drive means can be provided as gear
25 mechanisms, with a gear train connected to the drive motor and a gear-train output for each pump chamber. Although in this case the ratio of suction cycle to output cycle cannot be changed, the transport rate can be set very easily. The complexity involved here is likewise relatively slight.

30 In the following, preferred embodiments of the invention are described in greater detail with reference to drawings, wherein

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Fig. 1 is a schematic drawing of a first embodiment of the invention,

Fig. 2 is a diagram to explain the pump cycles,

5 Fig. 3 shows another embodiment of the invention in a drawing similar to Fig. 1,

Fig. 4 is a diagram to explain the pump cycles of the arrangement according to Fig. 3, and

Fig. 5 shows a third preferred embodiment of the invention.

10 In the following description, the same reference numerals are used for identical parts or parts with identical actions.

In the embodiment shown in Fig. 1 there are provided a first pump 20 and a second pump 30, each of which comprises a piston 25; 35, a cylinder 26; 36, a piston rod 27; 37, and a pump conduit 21 or 31 connected to a surgical instrument 1 by way of
15 output valves 24 and 34, respectively, and a clamp valve 2.

The pump conduits 21 and 31 are connected by way of suction conduits 22 and 32 and suction valves 23 and 33 to a suction conduit 12 that can be connected to a source 10 by way of a releasable coupling 11.

20 The piston rods 27 and 37 are releasably connected, by way of a first coupling 43 and second coupling 44, respectively, to a first motor 41 and second motor 42. The parts enclosed by the dashed line in Fig. 1 constitute a disposable unit, which is sterilized and placed in sterile packaging by the manufacturer
25 and is sent in this form to the merchant and/or end user.

The drive motors 41, 42 are connected to a control means (not shown) that controls the drive motors 41, 42 in such a way that the pistons 25, 35 travel along a path s , the time course of

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which is illustrated in Fig. 2. As shown in Fig. 2, the suction cycles, during which the quantity s increases (so that the curves for s rise in Fig. 2), are much shorter than the output cycles (during which the curves in Fig. 2 are falling).

5 Furthermore, the output cycles overlap in such a way that the sum of the volumes (defined by the pistons 25 and 35 as well as the cylinders 26 and 36) per unit time remains the same, with no decrease, so that a constant outflow of liquid from the source 10 to the surgical instrument 1 is ensured. As customary values for the pressure during employment in water-jet surgery, ca. 20 to 100 bar can be cited. Preferred stroke volumes of the pumps 20, 30 are between 2 and 100 ml per stroke.

15 The embodiment of the invention shown in Fig. 3 differs from that according to Fig. 1 primarily in that a third pump 50 with a third pump conduit 51, a third suction conduit 52, a third suction valve 53, a third output valve 54, a third piston 55, a third cylinder 56 and a third piston rod 57 are provided, as well as a third motor 45 and a third coupling 46 connected to the third piston rod 57.

20 In addition, in this embodiment of the invention the control means (not shown here) for the motors 41, 42 and 45 can be constructed so that the suction cycles are exactly as long as the output cycles, in which case the three cycles are arranged to be overlapping in such a way that again a uniform pump
25 output, i.e. pumped volume per unit time, is ensured. This is indicated schematically in Fig. 4, where the curves for the individual pumps 20, 30 and 50 are identified by these reference numerals.

30 The additional embodiment of the invention shown in Fig. 5 corresponds to the one in Fig. 3 except that no separate pump motors 41, 42 and 45 are provided. Instead the drive means 40 comprises a single motor 64, the shaft 65 of which is connected to a gear arrangement 60 comprising three gear mechanisms 61, 62 and 63, each of which drives a pump 20, 30 and 50,

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respectively. The gear mechanisms 61, 62 and 63 can be constructed, for example, as disk cam mechanisms, so that the actuation cycles can be arranged similarly to those according to Fig. 4. It is of course also possible to use a drive means
5 40 designed in this way with the embodiment according to Fig. 1.

List of reference numerals

	1	Surgical instrument
10	2	Clamp valve
	10	Source
	11	Coupling
	12	Suction conduit
	20	1st pump
15	21	1st pump conduit
	22	1st suction conduit
	23	1st suction valve
	24	1st output valve
	25	1st piston
20	26	1st cylinder
	27	1st piston rod
	30	2nd pump
	31	2nd pump conduit
	32	2nd suction conduit
25	33	2nd suction valve
	34	2nd output valve
	35	2nd piston
	36	2nd cylinder
	37	2nd piston rod
30	40	Drive means
	41	1st motor
	42	2nd motor
	43	1st coupling
	44	2nd coupling

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	45	3rd motor
	46	3rd coupling
	50	3rd pump
	51	3rd pump conduit
5	52	3rd suction conduit
	53	3rd suction valve
	54	3rd output valve
	55	3rd piston
	56	3rd cylinder
10	57	3rd piston rod
	60	Gear arrangement
	61	1st part of gear arrangement
	62	2nd part of gear arrangement
	63	3rd part of gear arrangement
15	64	Motor
	65	Shaft